

Optically addressable single-use microfluidic valves by laser printer lithography†

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We report the design, fabrication, and characterization of practical microfluidic valves fabricated using laser printer lithography. These optofluidic valves are opened by directing optical energy from a solid-state laser, with similar power characteristics to those used in CD/DVD drives, to a spot of printed toner where localized heating melts an orifice in the polymer layer in as little as 500 ms, connecting previously isolated fluidic components or compartments. Valve functionality, response time, and laser input energy dependence of orifice size are reported for cyclo-olefin polymer (COP) and polyethylene terephthalate (PET) films. Implementation of these optofluidic valves is demonstrated on pressure-driven and centrifugal microfluidic platforms. In addition, these “one-shot” valves comprise a continuous polymer film that hermetically isolates on-chip fluid volumes within fluidic devices using low-vapor-permeability materials; we confirmed this for a period of one month. The fabrication and integration of optofluidic valves are compatible with a range of polymer microfabrication technologies and should facilitate the development of fully integrated, reconfigurable, and automated lab-on-a-chip systems, particularly when reagents must be stored on chip for extended periods, *e.g.* for medical diagnostic devices, lab-on-a-chip synthetic systems, or hazardous biochemical analysis platforms.

1. Introduction

With many microfluidic technologies now maturing to the point where they could spur interesting commercial applications, an open question is whether these technologies are manufacturable in commercial volumes at economically viable costs; some authors claim that manufacturing costs are a principle obstacle in the commercialization of microfluidic devices.¹ In general, the more fabrication steps involved, the more expensive the manufacturing process. External support equipment and reagents needed to operate fluidic devices also drive system costs and, often more importantly, they can severely limit functionality and portability.² In nearly all demonstrations of microfluidic systems to date,^{2–9} microvalves—when they are included—have dictated to a lesser or greater extent the microfabrication and assembly steps and have often impacted functionality, flexibility, complexity, and cost as well.

Thermoplastic-based fluidic devices can be manufactured in large volumes at low cost through a diversity of well-established techniques, multilayer lamination, embossing and injection molding being the three most important.^{10–13} There have been a number of demonstrations of microfluidic systems in thermoplastics,^{10,11,14,15} but these examples are a rarity in academic research compared to microfluidic devices based on PDMS and glass.^{2,4,6,9,16–18} Arguably, integrated microfluidic devices based on PDMS and glass^{2–4,6,7,9} could be reconfigured as thermoplastic devices, but to date examples of this are few, and researchers continue to actively seek ways to improve or augment the function of glass-and-elastomer devices, only occasionally making the transition to thermoplastics.^{19–22} This trend can be explained in an academic research context by the low cost, simplicity, and rapidity of making masters from which to cast PDMS devices by a variety of methods available in many research labs, coupled with the wide availability of cleanroom facilities where glass microchannels can be patterned and etched. In contrast, injection molding or embossing have significantly higher tooling development costs and require molding equipment infrequently found in university microfabrication facilities. While low in cost for high-volume manufacture,¹ thermoplastic-based approaches are not necessarily optimal for academic research and prototyping.

Nonetheless, our belief is that the maturity of the field together with the importance of making the transition to commercial applications dictate that integrated microfluidic systems be designed from the outset with consideration of batch fabrication, volume manufacture, and reproducibility, and that this naturally leads to a preference for thermoplastic components and structures. Looking beyond manufacturing considerations, a range of biochemical techniques, including enzyme assays, various immunoassays, and the polymerase chain reaction, have been

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optimized for specific thermoplastic labware, as have numerous cell-based assays. Surface fouling and passivation against nonspecific adsorption, common problems in microfluidics, have been addressed previously for various thermoplastics used in 'macro' assays as well. Thus, microfluidic devices based on the same thermoplastic materials benefit from a large body of existing know-how.

An important recent trend is to operate microfluidic devices with the most inexpensive supporting instrumentation feasible,^{2,23} and this in turn has led to the "borrowing" of sophisticated but inexpensive consumer electronics technologies for lab-on-a-chip systems. For example, cell phones have been employed successfully to read the results of an assay run in a paper-based microfluidic device,²⁴ and "smartphones" can power some types of lab-on-chip systems, potentially analyzing and communicating the results as well.²⁵ In the area of detection, miniature fluorescence detection systems,²⁶ lens-free holographic imaging systems,²⁷ and adaptation of optical pickup and disc-spinning technologies from compact-disc and digital-video-disc hardware^{28,29} are examples of cleverly using affordable off-the-shelf consumer electronics components. Such approaches to capable but inexpensive systems could expedite the deployment of much-needed microfluidic-based diagnostic devices in developing nations²⁴ as well as developed countries.

The microfluidic valve is a ubiquitous, core component of microfluidic systems^{2-9,16,30} and its design, materials, and fabrication approach can greatly impact the cost-effective implementation of microfluidic systems. The microvalve controls fluid communication between fluidic elements such as microchannels, pumps, and reservoirs. Microvalves provide not only critical functionality, but also can, together with pumping mechanisms and detection approaches, dictate fabrication methods and operational protocols. The optofluidic valve we report here is an attempt to improve upon limitations of two of the most popular microfluidic valves, the elastomer diaphragm valve^{4,31,32} and the phase-change valve,^{3,33,34} which we briefly summarize.

In the elastomer diaphragm valve, a membrane, typically polydimethylsiloxane (PDMS), is sandwiched between a fluidic channel and a control channel, pressurization of which either closes or opens the fluidic channel. These devices comprise at least three layers (*e.g.*, PDMS/PDMS/glass); pressure to actuate the valves is typically controlled using mechanical screws or solenoids,^{35,36} pins from a Braille display,¹⁸ hydraulic means,³⁷ or, most popularly, air-pressure sources, again often controlled by electrical solenoid valves.^{4,16,31,32} Two key limitations of the PDMS diaphragm valve are (1) the need for often-bulky external components to actuate the valves, and (2) the high permeability of PDMS to water vapor as well as most organic solvents and compounds, making long-term (days to months) isolation of fluids, even aqueous buffer solutions, impractical.

Phase-change valves,^{3,33,34,38} in contrast, rely on a solid substance that, when heated, changes to a liquid state that can be displaced (or spontaneously displaces itself *via* capillary forces) to open or close a channel; actuation of these valves is accomplished with electric heaters^{3,20,33} or a laser beam.^{34,39} Two limitations of this valve are (1) the phase-change substance (*e.g.*, a wax such as paraffin) is in long-term direct contact with the solutions or reagents in its solid phase, and also contacts those liquids when in its molten state, and (2) the phase-change material must be

deposited, typically in molten form, in the microfluidic channel as part of the fabrication process, requiring a dedicated port or a heated-liquid dispense step in the device assembly process.

Both types of valve have been employed in several examples of microfluidic systems,^{2-9,16-18,38,40} and a combination of these two valve concepts has also been recently proposed.^{2,20} Other microvalves have been demonstrated including hydrogel valves,^{41,42} thermo-pneumatically actuated valves,⁴³ and electrophoretically permeable photopatterned gel valves.¹⁴ While droplet-based microfluidic architectures hold promise to drive complex assays without valves,⁴⁴ issues such as robustness to shock and vibration, evaporation, and compatibility with a wide range of liquid conductivities are still being addressed. Additional valve types have been proposed,^{45,46} but, as of yet, not implemented in microfluidic systems, perhaps owing to complexities of fabrication and assembly.

In this article, we introduce a new approach to the single-use ("one-shot") fluidic microvalve, based on laser printer lithography: an office laser printer precisely patterns dots of toner, on 100- μm thick thermoplastic substrates, which ultimately serve as the control elements of one-shot valves. The optofluidic valves are 'opened' with a single laser shot or pulse that is efficiently absorbed by the toner and quickly melts the underlying plastic film; the approach is compatible in terms of power, wavelength, and spot size with low-cost semiconductor diodes found in commercial DVD read/write drives. This technology is compatible with polymers and fabrication techniques such as hot embossing and multilayer plastic lamination. Compared to a similar approach that melts holes in plastic films without the aid of absorption by laser toner,⁴⁷ our approach requires lower laser powers (100–500 mW) and uses completely transparent foils, enabling addressing of valves on multiple fluidic levels. Laser positioning is less demanding since a general raster of the laser beam in the vicinity of the valve opens it without damaging the surrounding, unpatterned plastic film.

2. Concept

The optofluidic valve concept relies on the interaction of a laser beam with a toner-patterned polymer substrate as shown in Fig. 1. Most transparent foils transmit light in the visible and near-infrared regions of the spectrum: a laser beam passes almost unaffected through the substrate except for front-surface reflection and minor scattering. However, patterning a patch of an absorbing material on one side of the substrate alters the interaction of the beam with the substrate: if formed of an appropriate material, *e.g.* a black material with high optical density, the patch absorbs and converts the optical energy into thermal energy, which above some energy threshold melts and perforates the substrate. The patterning patch is realized by printing a dot with an office laser printer. Having a dot rather than the entire surface made from an absorbing material reduces the required accuracy of aiming the laser, provided it is scanned over an area that encompasses the valve dot.

3. Operation of optofluidic valves

This optofluidic valve principle was applied to the design and fabrication of microfluidic devices that require single-use

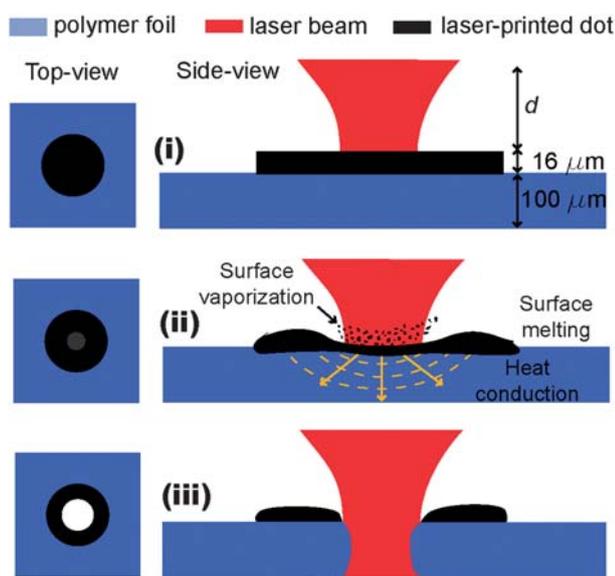


Fig. 1 Working principle of the one-shot optofluidic valve. (i) A dot patterned on a plastic substrate by a laser printer and a laser beam incident on that dot. (ii) The optical energy of the beam is converted into thermal energy with multiple consequences: surface vaporization, surface melting, and heat conduction through the plastic substrate. (iii) After 0.5 s, the plastic recedes, leaving an orifice. The distance d from the focal point was varied, as was the optical power level, to characterize the one-shot valves.

valves of the type shown in Fig. 2. The device consists of a single microfluidic “working layer” that includes and connects various fluidic components and modules. Fluidic continuity is interrupted in the working layer in places where valves are necessary; the working layer can include reservoirs with fluids stored for extended durations. The bottom layer is the microfluidic “connector layer,” containing a connecting microchannel in each location where segments of the working layer are to be (eventually) linked to one another. A plastic foil with laser-printed dots is sandwiched between these two layers. The foil underlying the dots can be perforated with a laser beam of appropriate power, connecting the separated regions of the working layer and allowing fluid to flow freely through. The valve must be designed in such a manner that bulk fluid is not in direct contact with the plastic in the region of the toner spot, as it would conduct away heat, preventing melting of the polymer foil. This is readily accomplished by the orientation of the fluidic device at time of valve opening and/or by placing the valve in a recessed feature where a small air bubble is trapped.

In another configuration of the optofluidic valve, the bottom microfluidic channel does not act as a connector *per se*, functioning instead as an independent microchannel that leads to other microfluidic elements or modules. In this case, only a single laser toner dot is required and just one orifice is created. Both configurations can be implemented in one device.

Note that the laser beam can be incident from either side of the microfluidic device, allowing the placement of the laser diode beneath or above the device according to convenience.

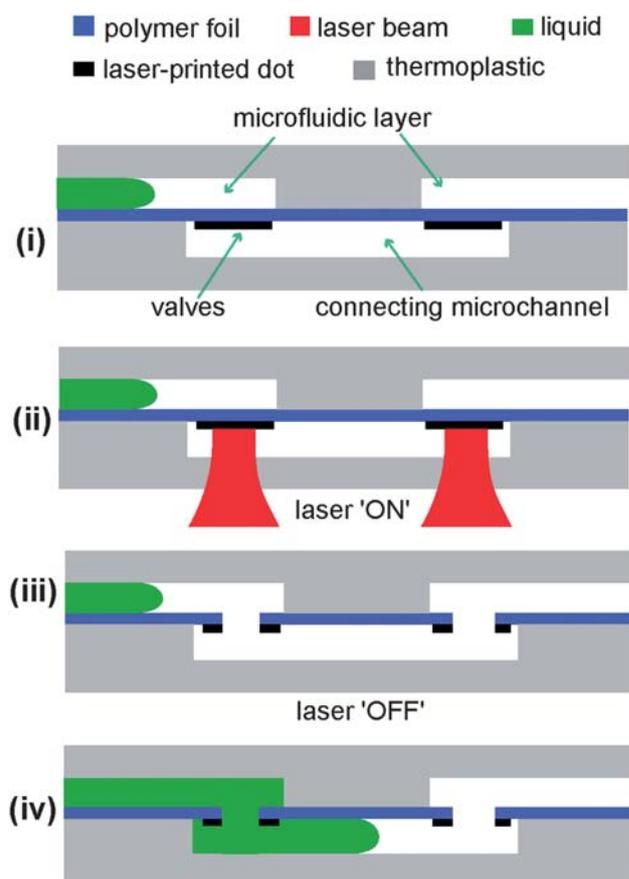


Fig. 2 Schematic of the microfluidic device operated with single-use valves. (i) A connecting microchannel in the bottom layer has two foil-blocked links to two channels in the upper microfluidic layer (i). Light from a laser beam melts orifices into the two valves (ii) opening them (iii). Liquid can flow from either upper channel, down through the connecting channel, and then into the other upper channel. Note that the laser beam can be incident from either side of the device.

4. Materials and methods

Fabrication

Valves (toner dots) were designed in Illustrator (v10, Adobe, USA) and printed on various plastic foils using an office laser printer (LaserJet 3030, HP, USA). Settings for the laser printer were chosen as ‘Transparency’ and ‘Prosser 1200’ for paper and print quality options, respectively. Several thermoplastic polymer foils were used as valve substrates: 125 μm -thick poly(methyl methacrylate), PMMA (GoodFellow, UK), 100 μm -thick polycarbonate, PC (Microfluidic ChipShop, Germany), 100 μm -thick cyclo-olefin polymer, COP (ZF14-100, Zeon Chemicals Europe, UK), and 100 μm -thick polyethylene terephthalate, PET (transparency films, CG3700, 3M, USA). These materials include some of the most-used thermoplastics in the fabrication of microfluidic devices.

For the demonstration of optofluidic valve prototypes, polymer foil substrates were manually cut to the size of the microfluidic module and attached to a sheet of paper using double-sided tape. The paper with the foil was then passed through the laser printer two times. The printer was allowed to cool for two minutes between printings.

Devices were fabricated using multilayer lamination. A CO₂ laser system (Laser Micromachining LightDeck, Optec, Belgium) was used to cut the various polymer layers. Connecting and microfluidic channels were cut from an 80- μm -thick layer of PSA (AR9808, Adhesives Research, Ireland) and laminated onto a 250 μm PMMA support layer (GoodFellow, UK) using a thermal roller laminator (Titan-110, GBC Films, USA).

Experimental setup

A 671 nm, 500 mW DPSS laser system (LSR-671-00400-03, OEM Laser Systems Inc, USA) was used to open the valves. DVD-RW players have similar power characteristics, see *e.g.* datasheet for GH16P40A8C, $\lambda = 660$ nm, 400 mW pulsed operation, Sharp, Japan. The laser system includes a diode driver with thermal control. An analog output module (NI 9264, National Instruments, USA) connected to an NI-Compact-DAQ chassis (NI CDAQ-9172) controlled the power output of the laser system.

The laser beam was focused onto microfluidic chips using an achromatic lens (F32-724, Edmund Optics, UK) with an effective focal length of 60 mm. Optical power of the laser was measured directly with a power meter (LaserCheck, Coherent, UK), see ESI, Fig. S1.†

Characterization

Light transmittance of plastics was measured with a UV-visible spectrophotometer (Cary 50, Varian, USA). Laser toner layer thickness was characterized with a scanning electron microscope, SEM (Evo LS 15, Zeiss, Germany). Orifice size was measured with a non-inverted microscope (Olympus).

5. Results and discussion

Optical spectra

Fig. 3 shows spectral transmission, from 200 to 800 nm, of the various plastics used in this study. Many plastics exhibit high transparency above 400 nm and throughout the visible spectrum,

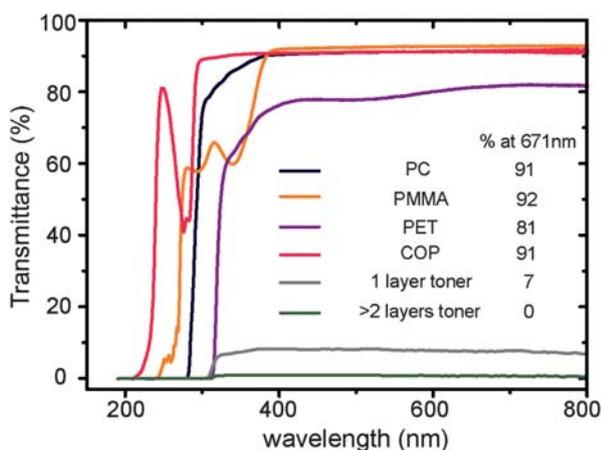


Fig. 3 Optical spectra of the different polymers employed to laser print dots. Single layer (gray) and double layer (green) laser-printing patterning on PET substrates.

including all of those we considered suitable for the laser valves, hence typical CD/DVD-power-level visible laser diodes could not be used to operate these valves in the absence of a light-absorbing spot. The effect of the number of black toner printed layers on the plastic was also investigated. For only one toner layer, 7% of light still passes through the film; for more than two printed toner layers, all the light is absorbed by the toner to the limit of detection of the spectrophotometer. Thus, in all subsequent experiments, plastic foils printed with two layers of black laser toner, which absorbs approximately 99% of the incident light, were used.

Printer toner composition and adhesion

The printed toner layer had a thickness of 16 μm for two layers. Typically, laser printer toner is mainly composed of a copolymer (45–55 wt%) and iron oxide (45–55 wt%),⁴⁸ as is the case for the print cartridge used in our experiments (Q2612A-L, HP, USA). The polymeric base of the toner is polystyrene (82%) and PMMA (18%) copolymer; it also includes amorphous silica (1–3 wt%). Some printer toners contain carbon black rather than iron oxide.⁴⁹ The resolution of the printer and the size of the toner particles will affect the thickness of the layer as well as its absorbance.^{48,50} Fused laser toner has been shown to be resistant to a variety of chemicals⁴⁸ and was utilized in the fabrication of polymeric microfluidic devices for electrophoresis, amperometric detection, and electrospray ionization.^{48,51}

The laser printer drum reaches temperatures up to 185 °C during printing.⁵² Many plastics at this temperature will melt or deform. Among the plastics we tested, only PET and COP 100- μm -thick substrates withstood these temperatures without deformation and with good adhesion of the toner to the substrate. Although PC has a high glass transition point (150 °C), toner particles did not adhere well to this substrate. PMMA substrates deformed when passed through the printer, although we noted that substrates > 250 μm did not deform as much as 100- μm -thick substrates, so it would be feasible to employ these materials. Other thermoplastics could be utilized as well, provided that they do not deform below 185 °C and that toner particles adhere to the plastic.

Orifice size and response times

Response times and orifice sizes were characterized at three different powers: 100, 300, and 500 mW; each power level was maintained continuously until the plastic melted sufficiently to form a hole. The effect of varying the distance of the plastic foil from the focal point in 5 mm increments (ESI, Fig S1†) was also investigated. Fig. 4 is a typical time-dependent response, showing three successive events, from a photodiode measuring scattered light during the characterization of one-shot laser valves on COP and PET substrates. Initially the laser is off and the signal from the photodiode is 0 V. Next, the laser is turned on and the beam strikes the plastic foil, producing maximum light scattering and driving the signal almost to the saturation voltage, –15 V. Once the plastic is perforated, the signal returns to almost 0 V because light scattering decreases to a very low value: most of the laser beam passes through the orifice unaffected.

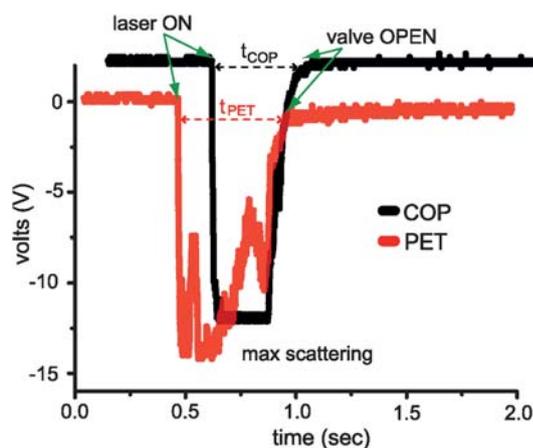


Fig. 4 Light-scattering-measured response time of the addressable optofluidic one-shot valves. Graph shows typical data from a photodiode (captured by an oscilloscope) for 100- μm -thick COP and PET substrates. Initially, the signal is constant at 0 V; when the laser is activated, the photodiode responds to scattered light and the signal increases almost to the saturation point. Once the valve has opened, typically in 500 ms or less, the signal returns close to 0 V, corresponding to minimal light scattering.

To obtain the response time of the valves, the time difference between laser beam turn-on and the return of the signal to a constant, near-baseline value was measured. Response time for the laser valves is constant at 0.5 s starting at a distance from the focal point of 5 mm for 300 and 500 mW laser powers (ESI, Fig S2 \dagger) for both plastic substrates, increasing to no more than 2.5 s at 100 mW. Of the distances tested, the response time of the valves is longest at the focal point (up to 10 s for PET substrates). Thus, optimum operation of the valves should start from a distance from the focal point of 5 mm and with powers greater than 300 mW.

For PET and COP, the orifice size increases as a function of the distance of the focal point from the plastic foil and of the laser power (ESI, Fig S3 \dagger). Orifice size for both substrates ranges from 32 μm to 278 μm , although bigger orifices should be achievable by further increasing the distance from the focal point. For both substrates, the orifice diameter is smaller than the theoretical laser beam waist except at the focal point, where the orifice size is almost the same as the focused beam, indicating that only part of the energy of the beam is used in the thermal ablation process. Similar results using low-power CO_2 lasers have been reported for PMMA.⁵³

Laser beam - plastic interactions

In contrast to UV laser micromachining, where the ablation of plastics occurs through a photochemical process, we believe the removal of plastic to open our optofluidic valves occurs through a photothermal ablation mechanism similar to CO_2 laser micromachining and to laser-welding of plastics.⁵⁴ The laser beam is absorbed at the surface of the laser-printed spot and the resultant thermal energy is conducted through the thickness of the material. The laser quickly heats the material to its melting point, then to its boiling point, and material is vaporized and

ejected. A solid-liquid interface is initially created, which moves away from the surface during the heating phase. The continuous laser irradiation causes a liquid-vapor interface to move through the material accompanied by removal of material through evaporation above the liquid-vapor interface.⁵⁴

Many thermoplastics have a decomposition temperature between 200–400 $^\circ\text{C}$.⁵⁵ An approximation of the surface temperatures generated with a Gaussian beam profile, T_{laser} , as in our laser system, can be calculated using the following expression:⁵⁶

$$T_{\text{laser}} = \frac{2P}{\pi^2 rK} + T_{\text{amb}} \quad (1)$$

where P is the laser power, r is the radius of the laser beam, K is the thermal conductivity, and T_{amb} is the ambient temperature. This equation implies that the laser energy is instantaneously converted to heat and entirely neglects any loss of heat, so it is only an upper bound, not an accurate estimate. The laser beam radius in our experiments varied from 32 μm to 243 μm . Thus, for PET, with $K = 0.24 \text{ W}/(\text{m K})$, the surface temperatures are calculated from 367 $^\circ\text{C}$ for the largest spot (243 μm) at 0.1 W to 13,213 $^\circ\text{C}$ for the smallest spot (32 μm) at 0.5 W. The latter temperature is highly unrealistic, as multiple thermal loss mechanisms, including conduction, boiling, and/or vaporization of the polymer would limit heating before the temperature exceeded a few hundred degrees. But even the lower temperature is enough to melt PET (260 $^\circ\text{C}$) and to initiate the decomposition (>300 $^\circ\text{C}$) of any PET that doesn't flow out of the beam. More realistic and detailed models⁵⁷ describe the different phase changes (melting, vaporization) that the foils undergo upon rapid heating and include heat loss, but eqn (1) is useful to set the upper bound based on power input to the material.

The gas pressure of the evaporating polymer can eject melted material. Fig. 5 shows an SEM image of a printed toner dot before and after laser opening of an orifice in the plastic. In Fig. 5(b), bulges are observed at the rim of the orifice; similar phenomena were reported by others when cutting with CO_2 lasers.^{53,58} These bulges are attributed to the ejection of molten polymer—from high-pressure gas (due to vaporization) or surface-tension-driven flow—that solidifies and accumulates on the rim when the material cools and meets air.^{53,58,59} This bulging could clog the microfluidic channel if the volume of melted/

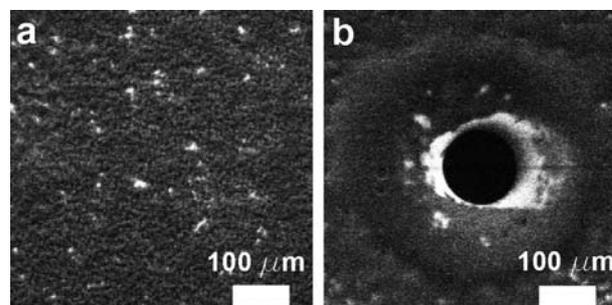


Fig. 5 (a) SEM image of a laser-printed spot on a PET substrate. (b) After a laser pulse melts the underlying plastic foil, creating an orifice that allows fluidic communication between two channels. Bulge formation at the rim of the orifice can be observed. Scale bars: 100 μm .

evaporated toner and polymer were sufficient to form a ‘bridge’ of molten material to the opposite layer of the microfluidic channel. In our devices, the 50- μm -deep channels were sometimes clogged by this effect, but for channels heights $> 150 \mu\text{m}$ all assembled devices were functional. The amount of material deposited at the rim of the hole depends on the thickness and properties of the plastic substrate and laser-toner layer, and should be considered in the design of microdevices based on these technologies.

It is possible that thermal decomposition products from the valve opening process could deposit on channel surfaces or diffuse through the channels, coming into contact with the fluid and possibly contaminating it. The laser-toner mixture of iron oxide and PMMA/polystyrene co-polymer (which, due to the toner fusing and thermal valve opening processes, may significantly encapsulate the iron oxide particles) have been shown to be inert to a variety of chemicals,⁴⁸ and the two copolymer constituents are themselves widely used in plastic labware. Furthermore, microfluidic electrophoretic separations in direct contact with the toner layer showed minimal effect on performance.⁵¹ Thus, effects of the toner itself on biological samples are expected to be minimal, although potential biocatalytic or redox effects of any unencapsulated iron oxide constitute potential concerns that warrant study; comparison with carbon-black-based toner could be informative if such effects are observed. The consequences of liquid contact with any thermal decomposition products are also of potential concern, requiring direct study and, ideally, chemical characterization of any thermal decomposition products formed as a function of supporting polymer film; toner spot diameter, thickness, and type; and valve opening parameters such as laser power density and duration. These effects will be the subject of future studies.

Given the high opening temperatures of the optofluidic valves, they must be designed such that bulk fluid is not in direct contact with the plastic in the region of the toner spot, as it would conduct away heat, preventing melting of the polymer foil. This is readily accomplished by the orientation of the fluidic device at the time of valve opening and/or by placing the valve in a recessed feature where a small air bubble is trapped.

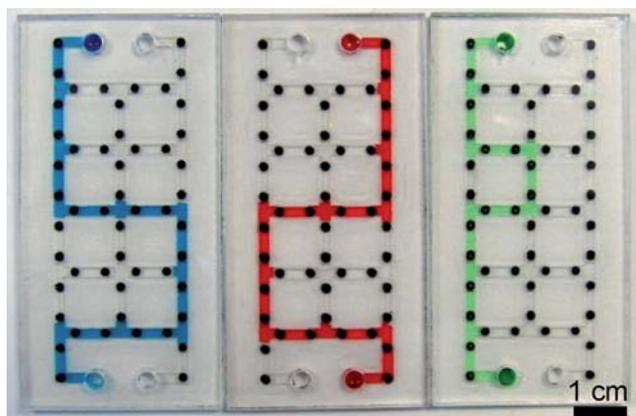


Fig. 6 Liquid microfluidic display. The display consists of three devices, each with two inlets and two outlets. After the device was assembled, 56 of the 106 optofluidic valves were opened to form the letters ‘bdi’.

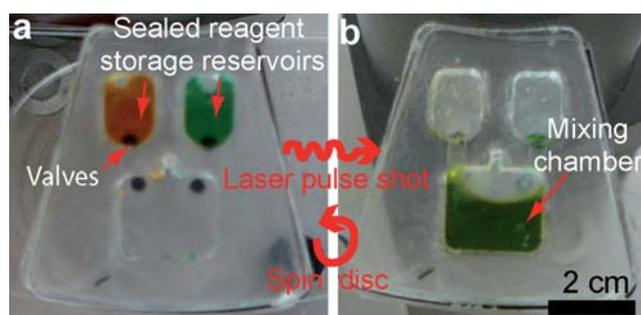


Fig. 7 A centrifugal microfluidic system consisting of two chambers connected by two channels to a mixing chamber. (a) Two colored solutions are initially loaded in two compartments and sealed to prevent evaporation. (b) After the laser valves are opened, the two solutions are forced into the mixing chamber by spinning the disc.

Microfluidic device examples

To demonstrate the optofluidic valve concept with powers similar to those used in DVD drives, we fabricated two different microfluidic devices. The first is a liquid microfluidic display, a matrix of 106 valves printed on a PET substrate that connects the microfluidic channel layer with the microfluidic connecting layer (ESI, Fig 4†). After the device was assembled, 56 of the valves were opened and a solution containing multiple colors of dye flowed through the channels, forming the letters ‘bdi’ as shown in Fig. 6. This type of device shows the potential for reconfigurable microfluidic devices, where individual paths could be formed depending on the desired assay steps or on the outcome of the previous valve configuration/reaction.

The second example device is a centrifugal microfluidic ‘lab-on-a-disc’ cartridge with two reservoirs connected to a mixing chamber through two independent microfluidic channels, Fig. 7. A solution is initially loaded into the reservoirs. The disc was rotated at a range of speeds and no leakage was observed through the valve even at 5000 rpm (the distance of the valve from the center of rotation is 3.2 cm, with an equivalent pressure of 100 kPa). The disc was then stopped, the laser diode beam was aimed in turn at each of the two toner dots, thereby creating a communicating port, and the disc was spun to move the two colored liquids into a mixing chamber. In a separate experiment, we showed that fluids can remain in isolated on-disc reservoirs for periods of 30 days (and undoubtedly much longer, but the measurement was ended at that time) without noticeable fluid loss. That demonstration used a COP device and film, selected in part for their low permeability to water vapor.

6. Summary and conclusions

We designed, fabricated, and characterized optofluidic valves. Using an office laser printer, toner dots that opto-thermally actuate the valves were deposited without damage on 100- μm -thick PET and COP foils. Response time of the valves on both substrates is on the order of half a second at 100 and 300 mW laser power; orifice sizes range from 30 to 280 μm at these powers. Thus, these optofluidic valves can be integrated with microchannels having widths of 50 μm or larger, and could work with smaller microchannels as well, given appropriate design

consideration of the potential for channel blockage by melted/ejected material. The valves open at power densities easily attainable with semiconductor diodes found in DVD R/W drives. Nevertheless, other visible semiconductor diodes such as those found in Bluray or CD players could also be used to open the valves.

Incorporation of these valves on microfluidic devices was also demonstrated and shown to be compatible with either pressure-driven or centrifugal microfluidic platforms. By forming the fluidic device from polymer layers rendered hydrophilic through appropriate surface chemical modification, this technology also could be used for capillary-flow-based devices.

This new laser-printed valve technology will facilitate the design and fabrication of fully integrated and automated lab-on-chip cartridges that require single-use valves, and in particular can, when combined with low-permeability materials of construction like COPs, enable long-term on-chip storage of aqueous buffers and reagents. The absence of mechanical components in the valve and its actuation process facilitate both its manufacture and use.

This technology can be adapted to multilevel microfluidics, where multiple layers of microfluidic channels are separated by multiple valving layers. As long as the laser-printed spots do not overlap, the appropriate valve can be selected on demand in any given layer, connecting channels on different layers at will.

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Electronic Supplementary Information

Optically Addressable Single-use Microfluidic Valves by Laser Printer Lithography

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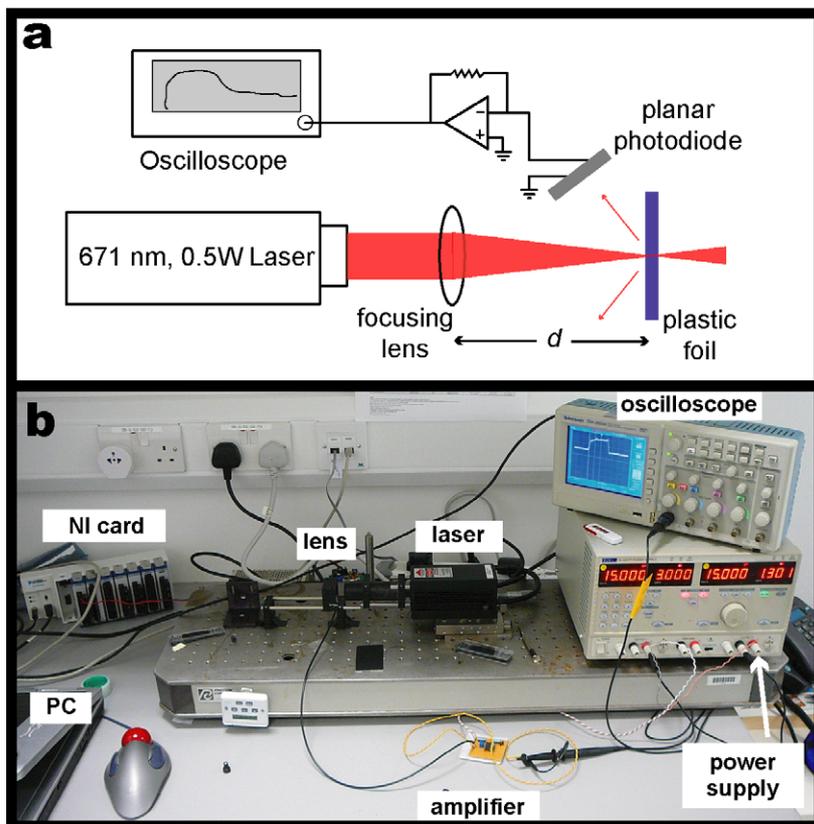
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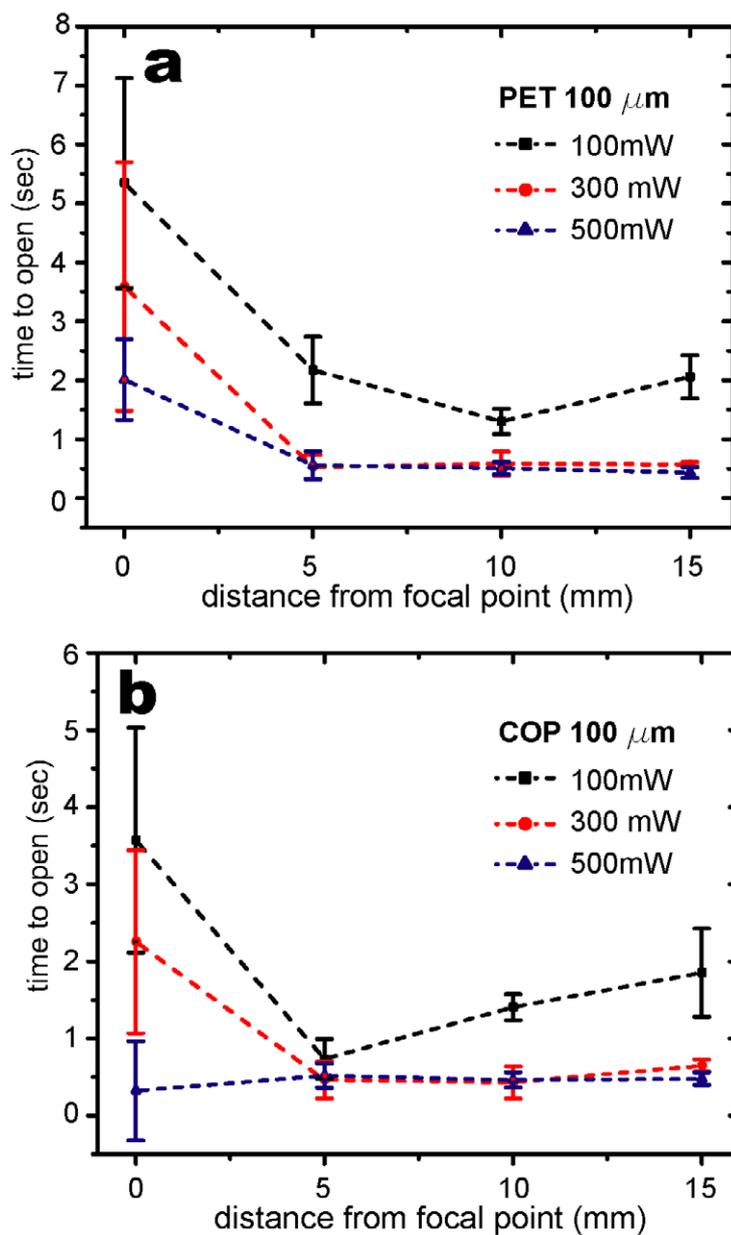
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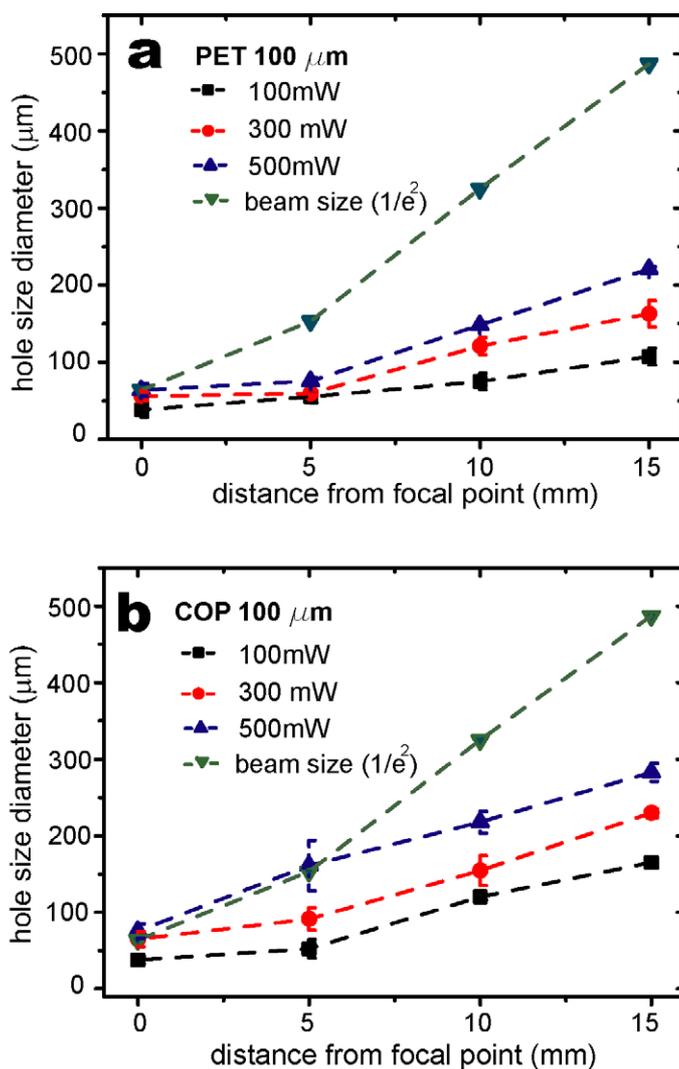
ESI Figure 1	S2
ESI Figure 2	S3
ESI Figure 3	S4
ESI Figure 4	S5



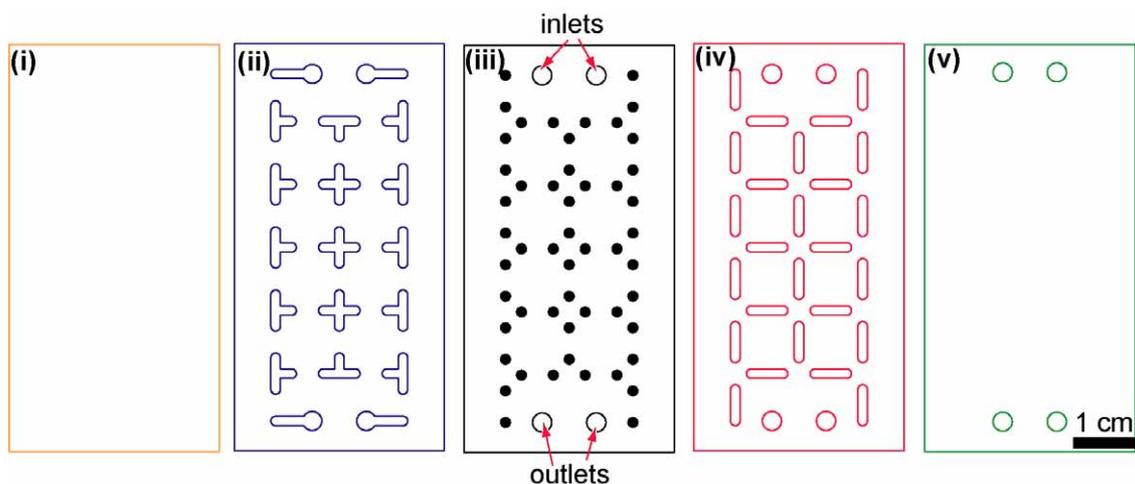
ESI_Figure 1. Schematic (a) and photograph (b) of the experimental setup. Light from a 671-nm solid-state laser system is focused onto a plastic foil with a lens. The distance d was varied to investigate the effect on the size of the orifice. Scattered light is measured using a planar photodiode connected to an oscilloscope through a transimpedance operational amplifier.



ESI_Figure 2. Valve response times. Results for 100- μm thick (a) PET and (b) COC substrates. Distance from the focal point, d , was varied from 0 to 15 mm. The opening time varied from 0.5 to 5.5 sec for PET, whereas for COC the time ranged from 0.25 to 3.5 sec.



ESI_Figure 3. Orifice size characterization on PET and COC substrates. The distance from the focal point, d , was varied from 0 to 15 mm. The laser valve orifice diameter varied from 30 μm to 225 μm for PET, whereas for COC the diameter ranged from 35 μm to 280 μm . The ray-tracing program TracePro (Lambda Research, USA) was employed to estimate the beam waist diameter at different distances from the focal point (achromatic lens, $f = 60$ mm, original laser beam diameter: 2 mm, beam divergence: 1 mrad). The beam diameter was defined where the intensity fell to $(1 - 1/e^2)$ of the maximum value (86% of the total beam energy).



ESI_Figure 4. CAD design of microfluidic device shown in Figure 6. The device consisted of 5 different laser-cut layers assembled by multi-layer lamination. The bottom substrate (i) consisted of a 500- μm thick layer of PMMA whereas the top substrate (v) consisted of a 1.2-mm thick PMMA layer. A laser printer was used to pattern dots on a PET substrate (iii). Inlets and outlets were manually cut in these layers. The microfluidic layer (ii) and the connecting microfluidic layer (iv) were composed of stacks of three layers: 50- μm double-sided PSA, 125- μm thick PC, and 50- μm double-sided PSA. Finally, the device was assembled by laminating these five layers together.